

# Ionic Mechanisms for Intrinsic Slow Oscillations in Thalamic Relay Neurons

A. Destexhe,<sup>\*,†</sup> A. Babloyantz,<sup>†</sup> and T. J. Sejnowski<sup>\*</sup>

<sup>\*</sup>The Howard Hughes Medical Institute and The Salk Institute, Computational Neurobiology Laboratory, La Jolla, California 92037 USA; and <sup>†</sup>Université Libre de Bruxelles, CP 231 Campus Plaine, Boulevard du Triomphe, B-1050 Bruxelles, Belgium

**ABSTRACT** The oscillatory properties of single thalamocortical neurons were investigated by using a Hodgkin-Huxley-like model that included  $\text{Ca}^{2+}$  diffusion, the low-threshold  $\text{Ca}^{2+}$  current ( $I_T$ ) and the hyperpolarization-activated inward current ( $I_h$ ).  $I_h$  was modeled by double activation kinetics regulated by intracellular  $\text{Ca}^{2+}$ . The model exhibited waxing and waning oscillations consisting of 1–25-s bursts of slow oscillations (3.5–4 Hz) separated by long silent periods (4–20 s). During the oscillatory phase, the entry of  $\text{Ca}^{2+}$  progressively shifted the activation function of  $I_h$ , terminating the oscillations. A similar type of waxing and waning oscillation was also observed, in the absence of  $\text{Ca}^{2+}$  regulation of  $I_h$ , from the combination of  $I_T$ ,  $I_h$ , and a slow  $\text{K}^+$  current. Singular approximation showed that for both models, the activation variables of  $I_h$  controlled the dynamics of thalamocortical cells. Dynamical analysis of the system in a phase plane diagram showed that waxing and waning oscillations arose when  $I_h$  entrained the system alternately between stationary and oscillating branches.

## INTRODUCTION

The thalamus is central to the generation of oscillatory activity during slow wave sleep. Two types of rhythmic activities of the electroencephalogram have been characterized, spindle waves (7–14 Hz) and delta waves (0.5–4 Hz). Spindle waves depend on both intrinsic and network mechanisms in the thalamus (Steriade and Deschenes, 1984; Steriade and Llinas, 1988). Until recently (Steriade et al., 1990) delta waves were assumed to originate in the cortex. However, a recent study conducted in cat in vivo (Curró Dossi et al., 1992; Nunez et al., 1992) showed that the thalamus can generate spontaneous oscillations of 0.5–4 Hz even after severing its connections with the cortex, which suggests an important thalamic contribution in the genesis of delta waves.

In vitro experiments on thalamocortical (TC) cells have demonstrated an intrinsic low-threshold  $\text{Ca}^{2+}$  spike (Jahnsen and Llinas, 1984a) and a tendency to oscillate. Cat and rat TC neurons display spontaneous slow oscillations in the delta range (Haby et al., 1988; Leresche et al., 1990, 1991; McCormick and Pape, 1990a) which are resistant to tetrodotoxin and therefore due to mechanisms intrinsic to the cell. These slow oscillations have also been called “pacemaker oscillations” (Leresche et al., 1990, 1991).

A waxing and waning oscillation was also found in cat TC cells in vitro (Leresche et al., 1990, 1991). These oscillations are composed of periods of 1.5–28 s of 0.5–3.2-Hz oscillation that wax and wane, separated by silent phases of 5–25-s duration. They are resistant to tetrodotoxin and are caused by mechanisms intrinsic to the TC neuron. By analogy with the

waxing and waning of in vivo spindles, they have been called “spindle-like oscillation” (Leresche et al., 1990, 1991). However in vivo spindles occur at a higher intraburst frequency (7–14 Hz) and depend on interactions with neurons of the thalamic reticular nucleus (Steriade and Deschenes, 1984; Steriade et al., 1985, 1987, 1990), so they are quite different from the waxing and waning slow oscillations studied here.

Electrophysiological investigations of the ionic mechanisms responsible for the intrinsic properties of TC neurons have revealed the presence of a low-threshold  $\text{Ca}^{2+}$  current,  $I_T$ , responsible for the generation of low-threshold spikes (LTS) following hyperpolarization (Deschenes et al., 1984; Jahnsen and Llinas, 1984b). More recently, voltage-clamp studies of this current in TC cells (Coulter et al., 1989; Crunelli et al., 1989; Huguenard and Prince, 1992) characterized the kinetic properties of  $I_T$  and the characteristic activation of this current in the subthreshold region of the membrane potential.

A mixed  $\text{Na}^+/\text{K}^+$  current,  $I_h$ , responsible for anomalous rectification, has also been identified in TC neurons studied in vitro (McCormick and Pape, 1990a; Pollard and Crunelli, 1988). The voltage-clamp technique has revealed that  $I_h$  is activated by hyperpolarization in the subthreshold range of potentials (McCormick and Pape, 1990a; Soltesz et al., 1991). This current was also shown to be involved in the generation of the slow oscillations of TC neurons (McCormick and Pape, 1990a; Soltesz et al., 1991) as well as in the state control of TC neurons by several neuromodulatory systems (McCormick and Pape, 1990a; McCormick and Williamson, 1991; Pape, 1992). The regulation of  $I_h$  can also control the transition between slow oscillations and waxing and waning oscillations in cat TC cells (Soltesz et al., 1991).

The purpose of the present paper is to investigate possible ionic mechanisms underlying the waxing and waning oscillations observed in single TC cells in vitro using a model of the TC neuron. The kinetic mechanisms in the model are

Received for publication 21 April 1993 and in final form 12 July 1993.

Address reprint requests to A. Destexhe at The Howard Hughes Medical Institute and The Salk Institute, Computational Neurobiology Laboratory, 10010 North Torrey Pines Road, La Jolla, CA 92037. Tel.: 619-453-4100 (ext. 527); Fax: 619-587-0417; e-mail: alain@helmholtz.sdsc.edu.

© 1993 by the Biophysical Society

0006-3495/93/10/1538/15 \$2.00

based on voltage-clamp data of  $I_T$  and  $I_h$ . Special emphasis is given to uncovering the role of  $I_h$  in organizing the transitions between multiple oscillatory and resting states of the TC cell.

## MATERIALS AND METHODS

Our single compartment model of a TC cell used a Hodgkin-Huxley-type scheme (Hodgkin and Huxley, 1952) for the ionic currents. The equation describing the derivative of the membrane potential  $V$  was:

$$C_m \dot{V} = -g_L(V - E_L) - I_T - I_h - I_{K2} + I_{ext}, \quad (1)$$

where  $C_m = 1 \mu\text{F}/\text{cm}^2$  is the specific capacity of the membrane,  $g_L = 0.05 \text{ mS}/\text{cm}^2$ , and  $E_L = -86 \text{ mV}$  are, respectively, the leakage conductance and the leakage reversal potential. The value of  $g_L$  was chosen to obtain a membrane time constant of 20 ms, and  $E_L$  was adjusted to match the resting membrane potential to  $-60 \text{ mV}$  (Jahnsen and Llinas, 1984a) when  $I_h$  was present, and to more hyperpolarized levels, when  $I_h$  was blocked (McCormick and Pape, 1990b). The total membrane area was assumed to be  $1000 \mu\text{m}^2$ , the area of a typical TC cell soma. Dendrites were not taken into account.

Only currents absolutely necessary to generate subthreshold oscillations were included in the model. These currents were the low-threshold  $\text{Ca}^{2+}$  current  $I_T$ , the hyperpolarization-activated current  $I_h$  and the voltage-dependent  $\text{K}^+$  current  $I_{K2}$ .  $I_{ext}$  represents the external current applied to the cell. Other  $\text{Na}^+$  and  $\text{K}^+$  currents, such as the  $I_{Na}$  and  $I_K$  responsible for the generation of action potentials,  $I_A$ ,  $I_{NaP}$ , or  $I_C$  were not included in the model (for details on these currents see McCormick and Huguenard, 1992).

Kinetic models have been developed previously for  $I_T$  (Huguenard and McCormick, 1992; Wang et al., 1991), for  $I_h$  (Destexhe and Babloyantz, 1993; Huguenard and McCormick, 1992), and  $I_{K2}$  (Huguenard and McCormick, 1992). We use them as our starting point.

### The low-threshold $\text{Ca}^{2+}$ current $I_T$

Voltage-clamp experiments (Coulter et al., 1989; Crunelli et al., 1989) show that the dynamical properties of  $I_T$  can be accounted for by a Hodgkin-Huxley-type formalism. A four-variable model of this low-threshold current was recently proposed by Wang et al. (1991) and will be used here. The kinetic equations read:

$$\begin{aligned} I_T &= -\bar{g}_{Ca} m^3 h (V - E_{Ca}) \\ \dot{m} &= -\frac{1}{\tau_m(V)} [m - m_\infty(V)] \\ \dot{h} &= \alpha_1(V) [1 - h - d - K(V)h] \\ \dot{d} &= \alpha_2(V) [K(V)(1 - h - d) - d], \end{aligned} \quad (2)$$

where  $\bar{g}_{Ca} = 1.75 \text{ mS}/\text{cm}^2$  is the maximum value of the conductance of the  $\text{Ca}^{2+}$  current and  $E_{Ca}$  is the  $\text{Ca}^{2+}$  reversal potential (in the presence of  $\text{Ca}^{2+}$  diffusion,  $E_{Ca}$  was calculated from the Nernst relation, and was taken as  $E_{Ca} = 120 \text{ mV}$  otherwise). In this kinetic scheme,  $m$  is the activation and  $h$  and  $d$  are two inactivation variables. The variable  $d$  accounts for the slow recovery of  $I_T$  from inactivation (Wang et al., 1991). The various functions used here are listed in Table 1.

### The hyperpolarization activated current $I_h$

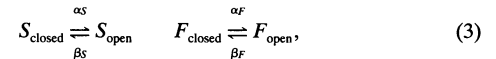
Voltage-clamp studies on thalamocortical neurons (McCormick and Pape, 1990a; Soltesz et al., 1991) have shown that  $I_h$  is a noninactivating current that activates slowly. This current is carried by both  $\text{Na}^+$  and  $\text{K}^+$  ions, and its reversal potential lies between  $E_{Na}$  and  $E_K$  (McCormick and Pape, 1990a).  $I_h$  activates in the same subthreshold range of membrane potentials as  $I_T$ .

**TABLE 1** Activation functions and time constants for the voltage-dependent currents  $I_T$ ,  $I_h$ , and  $I_{K2}$ .

Current	Variable	Function
$I_T$	$m$	$m_\infty(V) = 1/\{1 + \exp[-(V + 65)/7.8]\}$ $\tau_m(V) = 0.15m_\infty(V)\{1.7 + \exp[-(V + 30.8)/13.5]\}$
	$h$	$\alpha_1(V) = \exp[-(V + 162.3)/17.8]/0.26$ $K(V) = \sqrt{0.25 + \exp[(V + 85.5)/6.3]} - 0.5$
	$d$	$\alpha_2(V) = 1/\{\tau_2(V)[K(V) + 1]\}$ $\tau_2(V) = 62.4/\{1 + \exp[(V + 39.4)/30]\}$
	$S_1, F_1$	$H_\infty(V) = 1/\{1 + \exp[(V + 68.9)/6.5]\}$ $\tau_S(V) = \exp[(V + 183.6)/15.24]$ $\tau_F(V) = \exp[(V + 158.6)/11.2]/\{1 + \exp[(V + 75)/5.5]\}$
$I_{K2}$	$m2$	$m_{2\infty}(V) = 1/\{1 + \exp[-(V + 43)/17]\}$ $\tau_{m2}(V) = 2.86 + 0.29/\{\exp[(V - 81)/25.6] + \exp[-(V + 132)/18]\}$
	$h_1, h_2$	$h_{2\infty}(V) = 1/\{1 + \exp[(V + 58)/10.6]\}$
	$h_1$	$\tau_{h1}(V) = 34.65 + 0.29/\{\exp[(V - 1329)/200] + \exp[-(V + 130)/7.1]\}$
	$h_2$	$\tau_{h2}(V) = \tau_{h1}(V) \quad \text{for } V \geq -70 \text{ mV}$ $\tau_{h2}(V) = 2570 \text{ ms} \quad \text{for } V < -70 \text{ mV}$

These functions were chosen to fit voltage-clamp measurements of these currents. All values were scaled to a temperature of  $36^\circ\text{C}$  assuming  $Q_{10}$  values of 5 and 3 for  $I_T$  (Coulter et al., 1989), and of 2.6 for  $I_{K2}$  (Huguenard and Prince, 1991). The screening charge effect was calculated assuming an extracellular  $\text{Ca}^{2+}$  concentration of 2 mM.

Recently, a kinetic scheme for  $I_h$  was introduced to account for the kinetic properties of  $I_h$  (Destexhe and Babloyantz, 1993). Two distinct activation gates were assumed, namely  $F$  (fast activation) and  $S$  (slow activation) according to the following kinetic scheme:



where  $S_{\text{closed}}$  and  $F_{\text{closed}}$  represent the closed states of the slow and fast activation gates of  $I_h$ ,  $S_{\text{open}}$  and  $F_{\text{open}}$  represent the open states of these gates, and  $\alpha_S$ ,  $\beta_S$ ,  $\alpha_F$ , and  $\beta_F$  are voltage-dependent rate constants (see below).

The corresponding kinetic equations are:

$$\begin{aligned} I_h &= \bar{g}_h S_1 F_1 (V - E_h) \\ \dot{S}_1 &= \alpha_S(V) S_0 - \beta_S(V) S_1 \\ \dot{F}_1 &= \alpha_F(V) F_0 - \beta_F(V) F_1, \end{aligned} \quad (4)$$

where  $\bar{g}_h$  is the maximal conductance of  $I_h$  (in  $\text{mS}/\text{cm}^2$ ),  $E_h = -43 \text{ mV}$  is the reversal potential of  $I_h$  (McCormick and Pape, 1990a),  $S_0 = 1 - S_1$ , and  $F_0 = 1 - F_1$ .  $S_0$  and  $F_0$  represent the fraction of activation gates in the closed state, whereas  $S_1$  and  $F_1$  are the fraction of activation gates in the open state. The conductance of  $I_h$  is always proportional to the product  $S_1 F_1$  in this model.

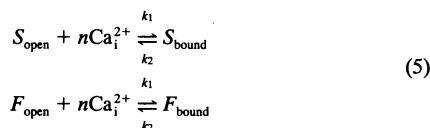
The rate constants are related to the activation function  $H_\infty(V)$  and the time constants  $\tau_S(V)$  and  $\tau_F(V)$  by the following relations:  $\alpha_S = H_\infty/\tau_S$ ,  $\beta_S = (1 - H_\infty)/\tau_S$ ,  $\alpha_F = H_\infty/\tau_F$  and  $\beta_F = (1 - H_\infty)/\tau_F$ . The activation function  $H_\infty(V)$  was chosen so that  $H_\infty^2$  fit the data of McCormick and Pape (1990a) (see Table 1). The time constants  $\tau_F(V)$  and  $\tau_S(V)$  (given in Table 1) were estimated from numerical simulation of voltage-clamp protocols (see Results).

### Regulation of $I_h$ by intracellular $\text{Ca}^{2+}$

Two plausible ionic mechanisms which produce waxing and waning oscillatory behavior are presented in Results. One possibility, initially pro-

posed by McCormick (1992), is the regulation of  $I_h$  by binding of intracellular  $\text{Ca}^{2+}$ , as found in whole cell voltage-clamp studies of  $I_h$  in sinoatrial node cells (Hagiwara and Irisawa, 1989). Evidence for the control of the voltage-dependent properties of  $I_h$  by intracellular  $\text{Ca}^{2+}$  were also obtained in cat neocortical neurons (Schwindt et al., 1992). As the  $\text{Ca}^{2+}$  dependence of  $I_h$  has not yet been studied in TC cells, it was assumed to be similar to that of sinoatrial node cells.

The activation curve of  $I_h$  in sinoatrial node cells shifts toward more positive potentials as the intracellular  $\text{Ca}^{2+}$  concentration ( $[\text{Ca}]_i$ ) is increased (Hagiwara and Irisawa, 1989). Calmodulin and protein kinase C were not involved in the  $\text{Ca}^{2+}$  modulation of  $I_h$ , suggesting that  $\text{Ca}^{2+}$  ions directly affected  $I_h$  channels (Hagiwara and Irisawa, 1989). There is also an increase of the conductance of  $I_h$  following the binding of  $\text{Ca}^{2+}$ . We have developed a kinetic model for intracellular calcium ( $\text{Ca}^{2+}$ ) binding to the open channels of  $I_h$  that is consistent with these data. The open state gates  $S_{\text{open}}$  and  $F_{\text{open}}$  were assumed to have  $n$  binding sites for  $\text{Ca}_i^{2+}$  which, when occupied, lead to the open forms  $S_{\text{bound}}$  and  $F_{\text{bound}}$  according to:



where  $k_1$  and  $k_2$  are the forward and backward rate constants for  $\text{Ca}_i^{2+}$  binding.

If  $S_2$  and  $F_2$  represent the fraction of gates bound to calcium, then, combining Eqs. 3 and 5, one obtains the following kinetic equations for  $I_h$ :

$$\begin{aligned} \dot{I}_h &= \bar{g}_h(S_1 + S_2)(F_1 + F_2)(V - E_h) \\ \dot{S}_1 &= \alpha_S(V)S_0 - \beta_S(V)S_1 + k_2[S_2 - CS_1] \\ \dot{F}_1 &= \alpha_F(V)F_0 - \beta_F(V)F_1 + k_2[F_2 - CS_1] \\ \dot{S}_2 &= -k_2[S_2 - CS_1] \\ \dot{F}_2 &= -k_2[F_2 - CF_1], \end{aligned} \quad (6)$$

where  $S_0 = 1 - S_1 - S_2$ ,  $F_0 = 1 - F_1 - F_2$ ,  $C = ([\text{Ca}]_i/\text{Ca}_{\text{crit}})^n$ , and  $\alpha_S$ ,  $\beta_S$ ,  $\alpha_F$ , and  $\beta_F$  were obtained from  $H_\infty$  and  $\tau_S$  as before. The number of binding sites was  $n = 2$  in all of our simulations. We assumed  $k_1 = k_2/\text{Ca}_{\text{crit}}^n = 5 \times 10^{-4} \text{ mM}$  is the critical value of  $[\text{Ca}]_i$  at which  $\text{Ca}^{2+}$  binding on  $I_h$  channels is half-activated (if  $[\text{Ca}]_i \ll \text{Ca}_{\text{crit}}$ , the effect of  $\text{Ca}_i^{2+}$  is negligible; see Results for the estimation of this parameter from voltage-clamp data).  $k_2 = 4 \times 10^{-4} \text{ ms}^{-1}$  is the inverse of the time constant of  $\text{Ca}_i^{2+}$  binding on  $I_h$  channels. These values were chosen to match the slow time course with which  $I_h$  is modulated by intracellular  $\text{Ca}^{2+}$ .

## Influx and efflux of $\text{Ca}^{2+}$

The dynamics of intracellular  $\text{Ca}^{2+}$  were determined by two contributions:

### (i) Influx of $\text{Ca}^{2+}$ due to $I_T$

$\text{Ca}^{2+}$  ions enter through  $I_T$  channels and diffuse into the interior of the cell. Only the  $\text{Ca}^{2+}$  concentration in a thin shell beneath the membrane was modeled. The influx of  $\text{Ca}^{2+}$  into such a thin shell followed:

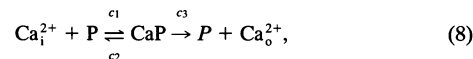
$$[\dot{\text{Ca}}]_i = -\frac{k}{2Fd} I_T, \quad (7)$$

where  $F = 96489 \text{ C mol}^{-1}$  is the Faraday constant,  $d = 1 \text{ } \mu\text{m}$  is the depth of the shell beneath the membrane, and the unit conversion constant is  $k = 0.1$  for  $I_T$  in  $\mu\text{A}/\text{cm}^2$  and  $[\text{Ca}]_i$  in millimolar.

### (ii) Efflux of $\text{Ca}^{2+}$ due to an active pump

In a thin shell beneath the membrane,  $\text{Ca}^{2+}$  retrieval usually consists of a combination of several processes, such as binding to  $\text{Ca}^{2+}$  buffers, calcium

efflux due to  $\text{Ca}^{2+}$  ATPase pump activity and diffusion to neighboring shells. Only the  $\text{Ca}^{2+}$  pump was modeled here. We adopted the following kinetic scheme:



where P represents the  $\text{Ca}^{2+}$  pump, CaP is an intermediate state,  $\text{Ca}_o^{2+}$  is the extracellular  $\text{Ca}^{2+}$  concentration, and  $c_1$ ,  $c_2$ , and  $c_3$  are rate constants.  $\text{Ca}^{2+}$  ions have a high affinity for the pump P, whereas extrusion of  $\text{Ca}^{2+}$  follows a slower process (Blaustein, 1988). Therefore,  $c_3$  is low compared to  $c_1$  and  $c_2$ , and the Michaelis-Menten approximation can be used for describing the kinetics of the pump. According to such a scheme, the kinetic equation for the  $\text{Ca}^{2+}$  pump is:

$$[\dot{\text{Ca}}]_i = -\frac{K_T[\text{Ca}]_i}{[\text{Ca}]_i + K_d}, \quad (9)$$

where  $K_T = 10^{-4} \text{ mM ms}^{-1}$  is the product of  $c_3$  with the total concentration of P, and  $K_d = c_2/c_1 = 10^{-4} \text{ mM}$  is the dissociation constant, which can be interpreted here as the value of  $[\text{Ca}]_i$  at which the pump is half activated (if  $[\text{Ca}]_i \ll K_d$  then the efflux is negligible).

The parameters of the pump were adjusted in order to have a fast  $\text{Ca}^{2+}$  removal, based on an estimation made from the time course of the spike after hyperpolarization in TC cells (McCormick and Huguenard, 1992). Slow  $\text{Ca}^{2+}$  handling is unlikely since  $\text{Ca}^{2+}$ -dependent channels would detect a slow  $\text{Ca}^{2+}$  accumulation in TC cells.

The extracellular  $\text{Ca}^{2+}$  concentration was  $[\text{Ca}]_o = 2 \text{ mM}$  as found in vivo. The change of  $[\text{Ca}]_i$  due to the binding of  $\text{Ca}^{2+}$  to  $I_h$  channels was negligible and was neglected, as was the contribution of  $\text{Ca}^{2+}$  efflux to the net  $\text{Ca}^{2+}$  current in Eq. 7.

The  $\text{Ca}^{2+}$  reversal potential strongly depends on the intracellular  $\text{Ca}^{2+}$  concentration, and was calculated according to the Nernst relation:

$$E_{\text{Ca}} = k' \frac{RT}{2F} \log \frac{[\text{Ca}]_o}{[\text{Ca}]_i}, \quad (10)$$

where  $R = 8.31 \text{ J mol}^{-1} \text{ K}^{-1}$ ,  $T = 309^\circ \text{ K}$ , and the constant for unit conversion is  $k' = 1000$  for  $E_{\text{Ca}}$  in mV. For  $[\text{Ca}]_i = 2.4 \times 10^{-4} \text{ mM}$ , which is an average value at rest in the simulations presented here,  $E_{\text{Ca}}$  was approximately 120 mV.

## Slow $\text{K}^+$ current $I_{K2}$

A second plausible ionic mechanism for the generation of waxing and waning oscillations depends on the interaction between three ionic currents, namely  $I_T$ ,  $I_h$ , and a slow outward current. Different types of  $\text{K}^+$  currents have been recently identified in TC cells (Budde et al., 1992; Huguenard and Prince, 1991; McCormick, 1991). Among these, a slowly inactivating  $\text{K}^+$  current activated by depolarization was characterized and termed  $I_{K2}$  by Huguenard and Prince (1991). They reported that this current inactivates very slowly with two time constants (around 250 ms and 3 s). A very similar current was found in TC cells in the lateral geniculate nucleus (McCormick, 1991). A kinetic model for this current was proposed by Huguenard and McCormick (1992):

$$\begin{aligned} I_{K2} &= \bar{g}_{K2} m_2 (0.6h_1 + 0.4h_2)(V - E_K) \\ \dot{m}_2 &= -\frac{1}{\tau_{m2}(V)} (m_2 - m_{2\infty(V)}) \\ \dot{h}_1 &= -\frac{1}{\tau_{h1}(V)} (h_1 - h_{1\infty(V)}) \\ \dot{h}_2 &= -\frac{1}{\tau_{h2}(V)} (h_2 - h_{2\infty(V)}) \end{aligned} \quad (11)$$

where  $\bar{g}_{K2}$  is the maximum value of  $I_{K2}$  conductance and  $E_K = -90 \text{ mV}$  is the reversal potential for  $\text{K}^+$  ions. The activation function and the time constant of the activation variables  $m_2$ ,  $h_1$ , and  $h_2$  are given in Table 1.

## Estimation of the values of parameters

Conductances values and reversal potentials for the above currents were estimated from published values provided by measurements *in vitro*. However, these data only provide approximate values for these parameters. Also, the complex dendritic geometry of the cell was not taken into account, which would affect these values. For each of the currents considered here, the value of the maximal conductance and the reversal potential are interrelated. For example, if  $E_h$  is increased,  $g_h$  must be decreased to reproduce similar results. We tested a broad range of maximal conductances and similar results were obtained.

## Methods for solving the equations

Exploration of the behavior of the system over a large range of values of the parameters was performed using programs developed specifically for the purpose of this paper, or by using the NEURON simulator (Hines, 1989, 1993). The solutions were obtained by direct integration of the differential equations using a fifth order, variable-step integration subroutine, provided by the CERN library (MERSON D208: accuracy of  $10^{-3}$ – $10^{-5}\%$ , minimal step reached  $10^{-1}$ – $10^{-3}$  ms). These solutions were rigorously identical to those obtained from the NEURON simulator (Euler integration, minimal step of  $10^{-1}$ – $10^{-2}$  ms).

The stationary states of the system (see Results) were calculated analytically, and the equations obtained were solved numerically by using a Newton-Raphson algorithm (Press et al., 1986). A confirmation of the value of the stationary state was also provided by direct integration of the differential equations.

The programs written for the purpose of this paper and the NEURON simulator were run on UNIX workstations (SONY NWS 3410 and MIPS 3000), and the typical time taken by a simulation of 10 s was of the order of 8–16 s CPU time.

## RESULTS

TC cells exhibit several types of slowly oscillating states in the subthreshold range of potentials (–60 to –80 mV). These oscillations were based on interactions between subthreshold currents, such as the low threshold  $\text{Ca}^{2+}$  current  $I_T$  and the hyperpolarization-activated current  $I_h$ . In particular, the mechanisms proposed here depend strongly on the kinetic properties of  $I_h$ . The parameters for  $I_h$  in our model were adjusted to fit voltage-clamp data.

### $\text{Ca}^{2+}$ and voltage-dependent activation of $I_h$

The activation function of  $I_h$  at equilibrium as a function of the membrane potential and the intracellular  $\text{Ca}^{2+}$  concentration is, from Eq. 6:

$$H_\infty(V, [\text{Ca}]_i) = [(S_1 + S_2)(F_1 + F_2)]_{\text{eq}} = \left[ \frac{1 + C}{H_\infty(V)^{-1} + C} \right]^2, \quad (12)$$

where  $C = ([\text{Ca}]_i / \text{Ca}_{\text{crit}})^n$ ,  $H_\infty(V)^2 = H_\infty(V, [\text{Ca}]_i = 0)$ . The activation function  $H_\infty(V, [\text{Ca}]_i)$  was determined from voltage-clamp measurements of TC neurons (McCormick and Pape, 1990a), and the parameters of  $H_\infty(V)$  were chosen to fit as closely as possible these data (Fig. 1 B, solid line).

Whole cell voltage-clamp experiments (Hagiwara and Irisawa, 1989) on sino-atrial node cells have shown that increasing intracellular  $\text{Ca}^{2+}$  produces a shift of the activation

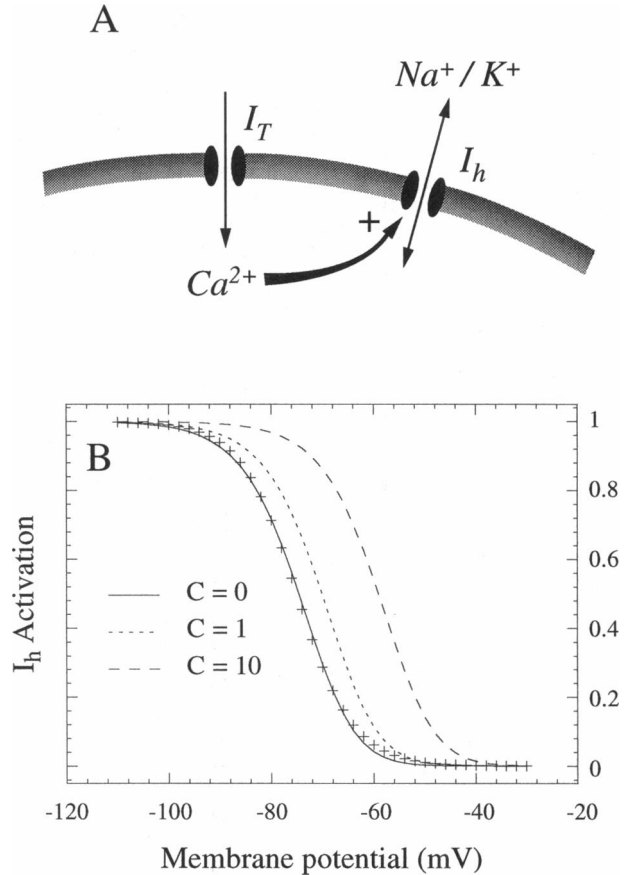


FIGURE 1  $\text{Ca}^{2+}$ -induced shift of the activation function of  $I_h$ . (A) Schematic diagram illustrating the currents in the model. The low-threshold  $\text{Ca}^{2+}$  current ( $I_T$ ) lets  $\text{Ca}^{2+}$  ions enter the cell; these ions bind to the mixed  $\text{Na}^+/\text{K}^+$  channel  $I_h$  and modify its voltage-dependent properties. (B) Direct binding of intracellular  $\text{Ca}^{2+}$  to  $I_h$  channels shifts the voltage dependence of the current toward positive membrane potentials.  $H_\infty(V, [\text{Ca}]_i)$  is represented as a function of the membrane potential  $V$  for different values of  $[\text{Ca}]_i$ . The activation function at resting level of  $[\text{Ca}]_i$  (solid line:  $C = 0$ ) was estimated from voltage-clamp experiments (McCormick and Pape, 1990a) on TC cells (+ symbols). For increasing concentrations of intracellular  $\text{Ca}^{2+}$ , the activation function shows progressively larger shifts toward positive membrane potential (dashed lines,  $C = 1$  and  $C = 10$ ).  $C = ([\text{Ca}]_i / \text{Ca}_{\text{crit}})^2$ .

function of  $I_h$  toward more positive membrane potentials. Using patch pipettes containing various concentrations in  $\text{Ca}^{2+}$ , the shift was around 13 mV for the highest concentrations in  $\text{Ca}^{2+}$  used.

These data can be accounted for by a kinetic scheme where intracellular  $\text{Ca}^{2+}$  directly binds to the  $I_h$  channels (see Fig. 1 A and Materials and Methods). The activation function  $H_\infty(V, [\text{Ca}]_i)$  progressively shifts toward positive membrane potentials as the value of  $C$  increases (Fig. 1 B).

The shift at half-activation of  $I_h$  is obtained by substituting  $H_\infty(V, [\text{Ca}]_i) = 0.5$  into Eq. 12, to obtain:

$$V_{1/2} = -68.9 + 6.5[\log(\sqrt{2} - 1) \log(C + 1)] \approx -75 + 6.5 \log \left[ \left( \frac{[\text{Ca}]_i}{\text{Ca}_{\text{crit}}} \right)^n + 1 \right]. \quad (13)$$

The shift of the  $I_h$  activation logarithmic in  $[Ca]_i$  and a shift of 13 mV is obtained for  $C = 6.4$ .

The shift should be negligible ( $C < 1$ ) at the resting level,  $[Ca]_i \sim 2 \times 10^{-4}$  mM, which gives a lower bound:  $Ca_{crit} > 2 \times 10^{-4}$  mM. During activation of  $I_T$ , the value of  $[Ca]_i$  just beneath the membrane increases to about  $10^{-2}$ – $10^{-3}$  mM and shifts  $I_h$  by a few millivolts ( $C > 1$ ), which gives an upper bound:  $Ca_{crit} < 10^{-2}$ – $10^{-3}$  mM. In the simulations presented here, we chose  $n = 2$  and  $Ca_{crit} = 5 \cdot 10^{-4}$  mM.

### Kinetics of $I_h$

$I_h$  activates very slowly and its time constant can be greater than 1 s at 3–6°C (McCormick and Pape, 1990a; Soltesz et al., 1991). The time course of  $I_h$  activation may differ considerably from the time course of deactivation at the same membrane potential. Currents similar to  $I_h$  in other preparations also show very slow activation and, in some cases, a faster time course for deactivation (for recent studies on  $I_h$ , see Erickson et al., 1993; Galligan et al., 1990; Kamondi and Reiner, 1991; Uchimura et al., 1990; van Ginneken and Giles, 1991; and references therein).

Despite the different time constants for activation and deactivation,  $I_h$  follows a single exponential time course, which would suggest a simple description involving first order kinetics. However, in a simple first-order kinetic scheme, the time constant of activation is identical to that of deactivation.

A novel kinetic scheme was proposed (Destexhe and Babloyantz, 1993) to account for these apparently conflicting experimental data (see Materials and Method). We assume that the permeability of  $I_h$  channels depends on two independent gates ( $S$  for slow activation and  $F$  for fast activation) which must be opened simultaneously.

This model exhibits two time constants. Following a depolarizing voltage jump, the two gates  $S$  and  $F$ , which are initially closed, begin to activate: the fast variable  $F_1$  rapidly increases to its equilibrium value, whereas  $S_1$  reaches the same value more slowly. Since  $I_h$  is proportional to the product  $S_1 F_1$ , the time course of the measured current will reflect the activation kinetics of the slow variable  $S_1$  (Fig. 2 A). The opposite occurs upon a hyperpolarizing voltage jump from a depolarized level where both gates were initially open:  $F_1$  rapidly closes, while  $S_1$  closes more slowly. Since the decrease of  $F_1$  immediately decreases  $I_h$ , the time course of deactivation follows the kinetics of the fast variable (Fig. 2 B).

Although in our model for  $I_h$  the current is a product of two exponentials (Eq. 4), the two time constants were sufficiently different that the time course of the current was practically a single exponential. This could explain the single exponential curves observed from voltage-clamp experiments of  $I_h$ .

The slow time constant,  $\tau_S(V)$ , was chosen by an exponential fit of voltage-clamp measurements of the time constants of activation, whereas the fast time constant,

$\tau_F(V)$ , was fit by a bell-shaped function from measurements of the deactivation time constants (see Fig. 2 C and Table 1).

Simulation of voltage-clamp experiments using these functions produced curves and measurements indistinguishable from those obtained by McCormick and Pape (1990a) (Fig. 2 C). In particular, the double activation scheme for  $I_h$  deactivates faster than it activates (Destexhe and Babloyantz, 1993).

In the next section, regulation of  $I_h$  by  $Ca^{2+}$  is introduced and its interactions with other currents examined.

### Oscillatory behavior from $Ca^{2+}$ -regulated $I_h$

Previous models of TC cells have shown that the interaction between  $I_T$  and  $I_h$  supports slow oscillations in the delta range 0.5–4 Hz (Lyttton and Sejnowski, 1992; McCormick and Huguenard, 1992; Toth and Crunelli, 1992a). We demonstrate here that this slow oscillation can wax and wane as a result of the interaction between the two subthreshold currents  $I_T$  and  $I_h$ , and the regulation of  $I_h$  by intracellular  $Ca^{2+}$ .

The double activation model of  $I_h$  combined with  $I_T$  can give rise to a variety of resting states and slow oscillations. These patterns were obtained for different values of the maximal conductance  $\bar{g}_h$  of  $I_h$  (Fig. 3). For the lowest values of  $\bar{g}_h$  ( $< 0.01$  mS/cm<sup>2</sup>), the model remained in a hyperpolarized resting state at about –84 mV (Fig. 3 A). A similar hyperpolarized resting state has been observed in vitro (McCormick and Pape, 1990a; Soltesz et al., 1991) after blockage of  $I_h$ .

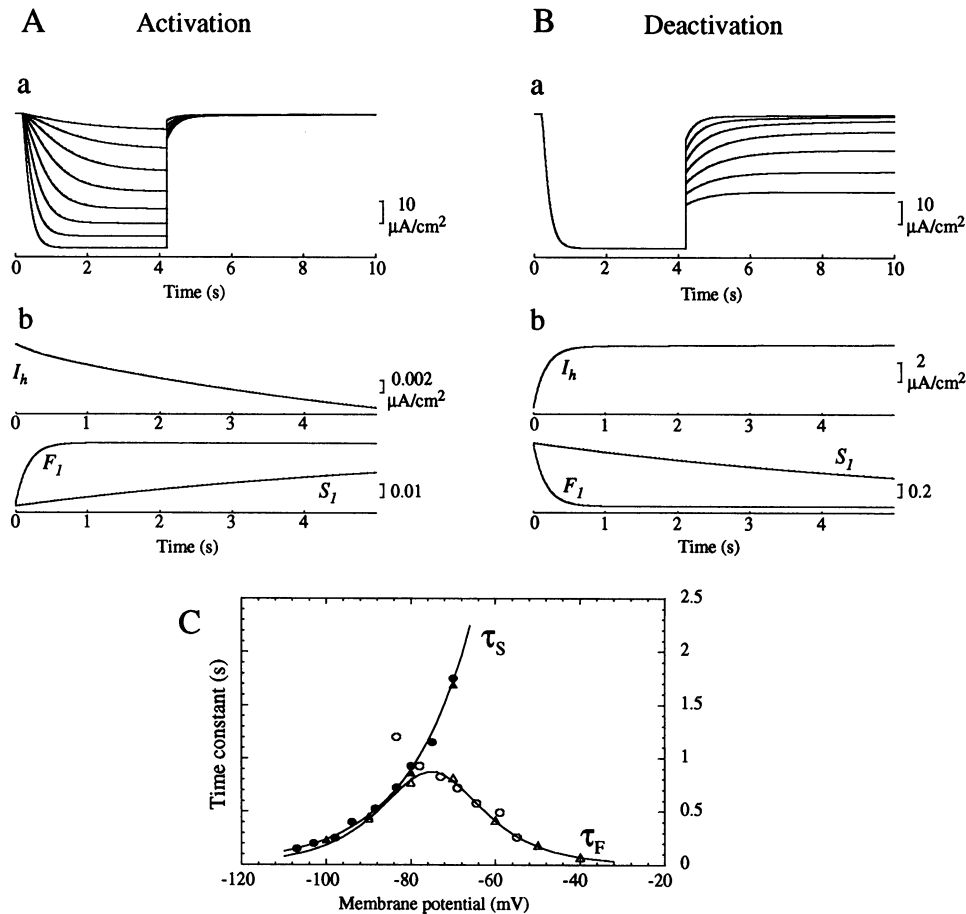
For the highest values of this conductance ( $\bar{g}_h > 0.1$  mS/cm<sup>2</sup>), there was a more depolarized resting state (around –58 mV) close to firing threshold (Fig. 3 D). The depolarized resting state was similar to that observed in vitro following the enhancement of  $I_h$  by noradrenaline and probably corresponds to the “relay state” of TC neurons (McCormick and Pape, 1990a; Soltesz et al., 1991).

For moderate values of  $\bar{g}_h$ , various types of slow oscillatory behavior were observed. In the range of  $\bar{g}_h$  between 0.0018 and 0.02 mS/cm<sup>2</sup>, there was a regular slow oscillation of 0.5–3.5 Hz (Fig. 3 B) similar to the slow oscillatory behavior recorded in TC cells in vitro (McCormick and Pape, 1990a).

For somewhat higher values of  $\bar{g}_h$  (between about 0.02 and 0.09 mS/cm<sup>2</sup>), waxing and waning oscillations appeared (Fig. 3 C) that consisted of bursts of slow oscillations (typically lasting a few seconds at frequency of 3.5–4 Hz with faster components at 8–9 Hz) separated by a silent phases lasting about 4–20 s. Such bursts of slow oscillations (0.5–3.2 Hz) separated by silent phases (5–25 s) have been recorded in cat TC cells in vitro (Leresche et al., 1990, 1991).

### Properties of $Ca^{2+}$ -dependent waxing and waning oscillations

Soltesz et al. (1991) showed that slow oscillations and waxing and waning oscillations observed in cat TC cells are two



**FIGURE 2** Activation and deactivation kinetics of  $I_h$ . (A) Simulation of voltage-clamp protocols of activation of  $I_h$ . (a) From an initial holding value of  $-55$  mV, the voltage was clamped at various levels (from  $-105$  to  $-70$  mV) for 4 s, then clamped again to  $-55$  mV. (b) Time course of the current compared to the gating variables. During this activation protocol (initial voltage of  $-30$  mV, current recorded after clamping to  $-50$  mV at  $t = 0$ ) the current follows the time course of the slow variable  $S_1$ . A time constant of about 3 s was estimated from fitting a single exponential to the current trace. (B) Simulation of protocols of deactivation of  $I_h$ . (a) The voltage was clamped at  $-105$  mV for 4 s, then clamped to various levels from  $-85$  to  $-55$  mV. (b) Time course of the current and gating variables. In this case, although the voltage was clamped to the same value as in Ab (initial voltage of  $-110$  mV and clamp to  $-50$  mV at  $t = 0$ ), the current followed the time course of the variable  $F_1$  and a smaller time constant of about 180 ms was measured. (C) Time constants for activation and deactivation of  $I_h$  as a function of the membrane potential. The time constants obtained by single-exponential fitting of the currents illustrated above for activation (filled triangles) and deactivation (open triangles) were compared to the measurements obtained by McCormick and Pape (1990a) during activation (filled circles) and deactivation (open circles). Solid lines represent the functions fit to these data (given in Table 1). Adapted from Destexhe and Babloyantz (1993).

states in a continuum and that the transition from slow oscillations to waxing and waning type of rhythmicity could be achieved by enhancement of  $I_h$ . The same sequence of oscillations was observed here as  $I_h$  was enhanced in the model (Fig. 3). Other properties of *in vitro* waxing and waning oscillations include a characteristic hyperpolarization during the silent phase and their transformation into slow oscillations by a depolarizing current step. These properties were also present in our model (Fig. 4, A and B).

The transition from waxing and waning oscillation to slow oscillations from a depolarizing current step was not observed for all values of  $\bar{g}_h$ . For some values of  $\bar{g}_h$ , the opposite was observed: waxing and waning oscillations were transformed into slow oscillations by applying a hyperpolarizing current step (not shown).

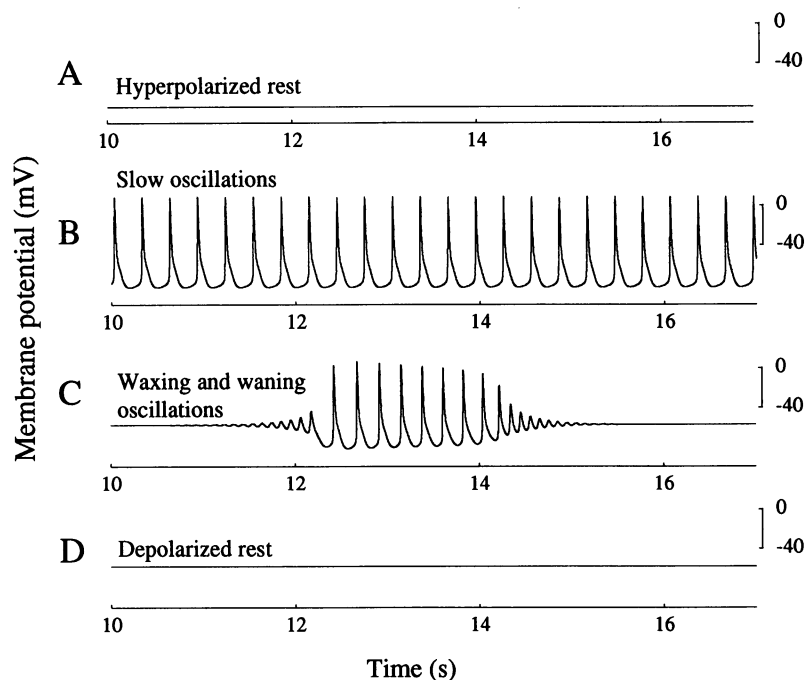
There was a progressive hyperpolarization during the silent phase (Fig. 4 B). During the burst there was a gradual

depolarization that was most clearly seen by averaging the membrane potential (Fig. 4 C).

The time courses of the different variables of the model during a waxing and waning sequence are displayed in Fig. 5. The membrane hyperpolarized slowly during the silent phase until  $I_T$  deinactivated and the oscillations began. During the burst of slow oscillations,  $\text{Ca}^{2+}$  entered transiently at the peak of each spike and bound progressively to  $I_h$  channels (reflected in the slow increase of  $S_2$  and  $F_2$ ).  $\text{Ca}^{2+}$  binding to  $I_h$  channels shifted the  $I_h$  activation curve, producing a gradual depolarization during the oscillatory phase (Fig. 4 C). This depolarization prevented  $I_T$  from activating and damped the slow oscillations. During the ensuing silent phase,  $S_2$  and  $F_2$  slowly decreased and caused the membrane to hyperpolarize.

The progressive transformation of slow oscillations into waxing and waning oscillations is shown in Fig. 6. A bifur-

FIGURE 3 Resting states and slow oscillations in the presence of  $I_T$  and  $\text{Ca}^{2+}$ -dependent  $I_h$  obtained at four values of the maximal conductance of  $I_h$ . (A) Hyperpolarized resting state close to  $-84$  mV for  $\bar{g}_h = 0$ . (B) Slow oscillations of about 3.5 Hz for  $\bar{g}_h = 0.01$  mS/cm<sup>2</sup>. (C) Waxing and waning oscillations of about 4–8 Hz for  $\bar{g}_h = 0.04$  mS/cm<sup>2</sup>. (D) Depolarized resting state around  $-58$  mV for  $\bar{g}_h = 0.11$  mS/cm<sup>2</sup>. The maximum conductance of  $I_T$  was kept fixed at  $\bar{g}_{Ca} = 1.75$  mS/cm<sup>2</sup>.



cation occurred around  $\bar{g}_h = 0.02$  mS/cm<sup>2</sup> from slow oscillations to a state where the slow oscillations were interrupted by short silent phases (Fig. 6 B). As  $\bar{g}_h$  increased, the length of the silent phase increased and the bursts became shorter (Fig. 6, C and D). The frequency inside the oscillatory phase was always comparable to that of the slow oscillations.

The duration of the silent phase and the oscillatory phase as a function of  $\bar{g}_h$  are reported in Fig. 7 A. The silent phase ranged from 4 to 20 s and decreased with  $\bar{g}_h$ . The oscillatory phase became shorter with increase of  $\bar{g}_h$ . In the limit, as  $\bar{g}_h$  decreased to 0.02 mS/cm<sup>2</sup>, the duration of oscillatory phase tended to infinity. The opposite oc-

curred as the depolarized state was approached, with oscillatory phase reducing to a minimum length before disappearing (sometimes a low amplitude periodic oscillation was seen in a very narrow range of  $\bar{g}_h$  before the depolarized state appeared). The period of the slow oscillation decreased with  $\bar{g}_h$  (indicated by  $S$  in Fig. 7 A), which is consistent with the slowing down of the slow oscillation observed after progressive blockage of  $I_h$  channels by cesium (McCormick and Pape, 1990a).

The length of the silent phase and of the oscillatory phase were directly proportional to the time constant of intracellular  $\text{Ca}^{2+}$  binding to  $I_h$  channels,  $k_2^{-1}$  (Fig. 7 B). This is

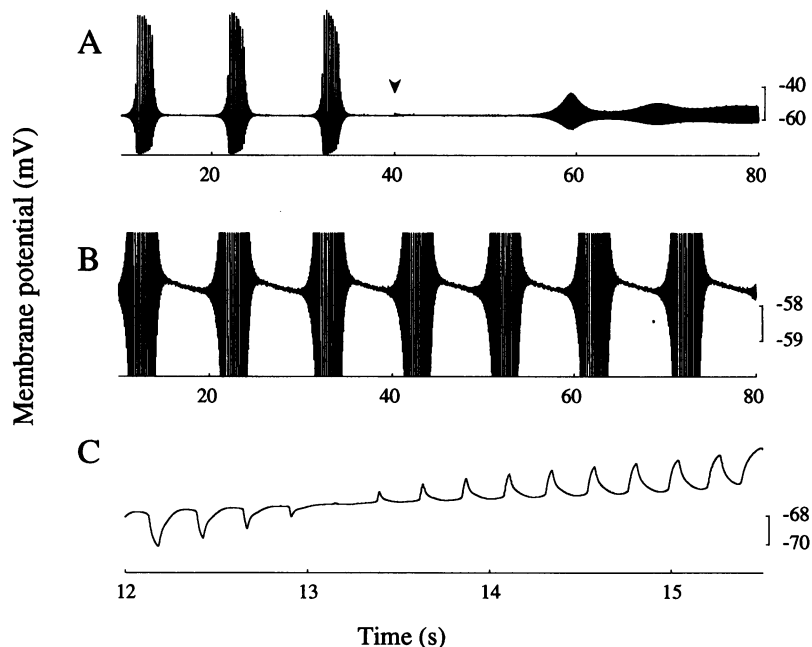


FIGURE 4 Properties of  $\text{Ca}^{2+}$ -dependent waxing and waning oscillations. (A) Transformation of waxing and waning oscillations into slow oscillations by application of a depolarizing current step of  $0.05 \mu\text{A}/\text{cm}^2$  (arrow).  $\bar{g}_h = 0.04$  mS/cm<sup>2</sup>. (B) Waxing and waning oscillations at high amplification showing the slow hyperpolarization of the membrane during the silent phase.  $\bar{g}_h = 0.04$  mS/cm<sup>2</sup>. (C) Average membrane potential showing a progressive depolarization during the oscillatory phase. Each point was obtained by averaging the membrane potential over a period of 500 ms.  $\bar{g}_h = 0.025$  mS/cm<sup>2</sup>.

consistent with the assumption that the binding of  $\text{Ca}^{2+}$  is critical for the onset and termination of the oscillatory phase. The silent phase, which depends on the return of  $S_2$  and  $F_2$  to their resting values, is expected to be proportional to  $k_2^{-1}$ . The length of the oscillatory phase, which depends on the rate of rise of  $S_2$  and  $F_2$ , is also expected to be proportional to  $k_2^{-1}$ .

### $I_{K2}$ -dependent waxing and waning oscillations

The  $\text{Ca}^{2+}$ -dependent regulation of  $I_h$  is not the only way to obtain waxing and waning oscillation with  $I_T$  and  $I_h$ . A second possible mechanism depends on the interaction among  $I_T$ ,  $I_h$ , and the slow  $\text{K}^+$  current  $I_{K2}$ .  $\text{Ca}^{2+}$  mechanisms were not included in this version of the model.

It was reported previously (Destexhe and Babloyantz, 1993) that the double activation model of  $I_h$  showed the same sequence of oscillatory states as in vitro experiments when combined with  $I_T$  and  $I_{K2}$ . This model was explored using different values for some of the parameters. Characteristic properties of waxing and waning oscillations, such as the progressive hyperpolarization during the silent phase and the transformation into slow oscillations by applying a depolarizing current step, were also observed in this model (Fig. 8).

Fig. 9 shows the time course of several gating variables during a waxing and waning sequence. As in the mechanism proposed by Soltesz et al. (1991),  $I_h$  activates more and more

during each cycle of the oscillatory phase. The resulting depolarization inactivates  $I_T$  and the oscillations damp.

Compared with the  $\text{Ca}^{2+}$ -dependent waxing and waning oscillations, the slow depolarization of the membrane during the oscillatory phase in the  $I_{K2}$ -dependent model is provided by a more pronounced  $I_h$  activation ( $S_1$  reaches its maximal value during the oscillatory phase) and inactivation of  $I_{K2}$ . Progressive deactivation of  $I_h$  then hyperpolarizes the membrane.

Waxing and waning oscillations were never observed without adding a slow depolarization-activated outward current in addition to  $I_T$  and  $I_h$ . Similar oscillations were observed when  $I_{K2}$  was replaced by slow  $\text{K}^+$  currents, such as the slow  $\text{Ca}^{2+}$ -activated  $\text{K}^+$  current or a depolarization-activated noninactivating  $\text{K}^+$  current similar to the muscarinic current  $I_M$  (not shown). However, these currents are probably not present in TC cells.

### Singular approximation of waxing and waning oscillations

Instead of studying the mechanisms of waxing and waning oscillations in terms of activation variables and  $\text{Ca}^{2+}$  concentration, it is possible to describe these oscillations as *dynamical states* of the system. This provides a more global view of “stationary states” or “limit cycle oscillations” of the system. Complex oscillatory processes, such as oscillations

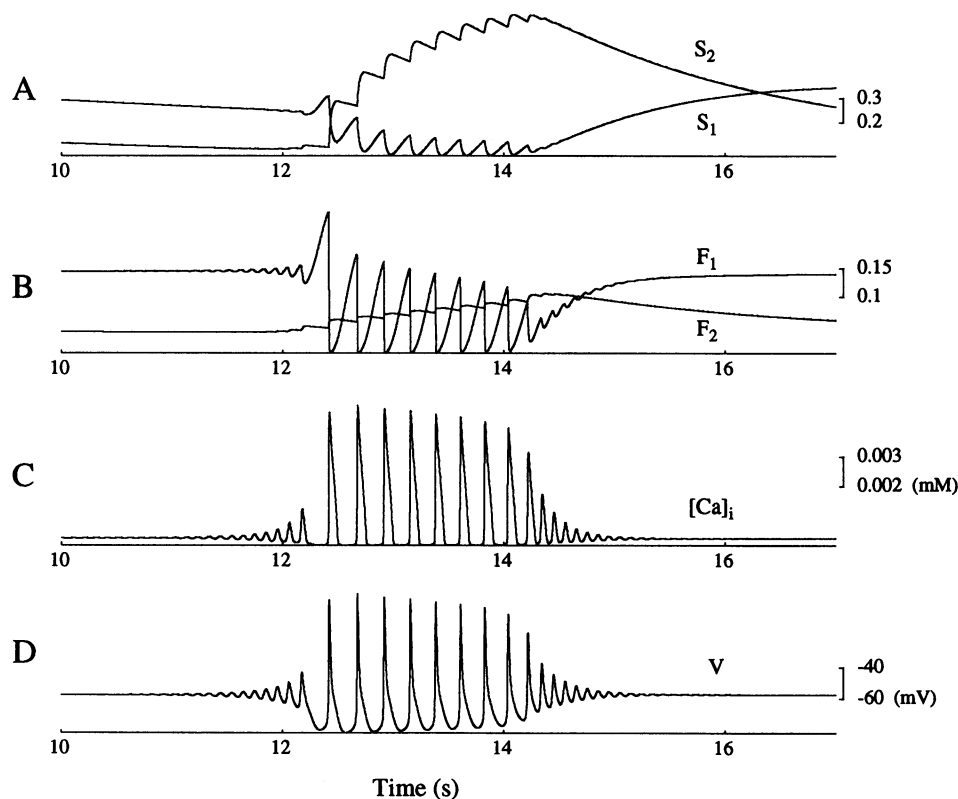


FIGURE 5 Time course of the gating variables of  $I_h$  during  $\text{Ca}^{2+}$ -dependent waxing and waning oscillations. (A) Slow activation variables  $S_1$  and  $S_2$ . (B) Fast activation variables  $F_1$  and  $F_2$ . (C) Intracellular  $\text{Ca}^{2+}$  concentration  $[\text{Ca}]_i$ . (D) Membrane potential  $V$ .  $\bar{g}_h = 0.04 \text{ mS/cm}^2$ . Same parameters as in Fig. 3 C.



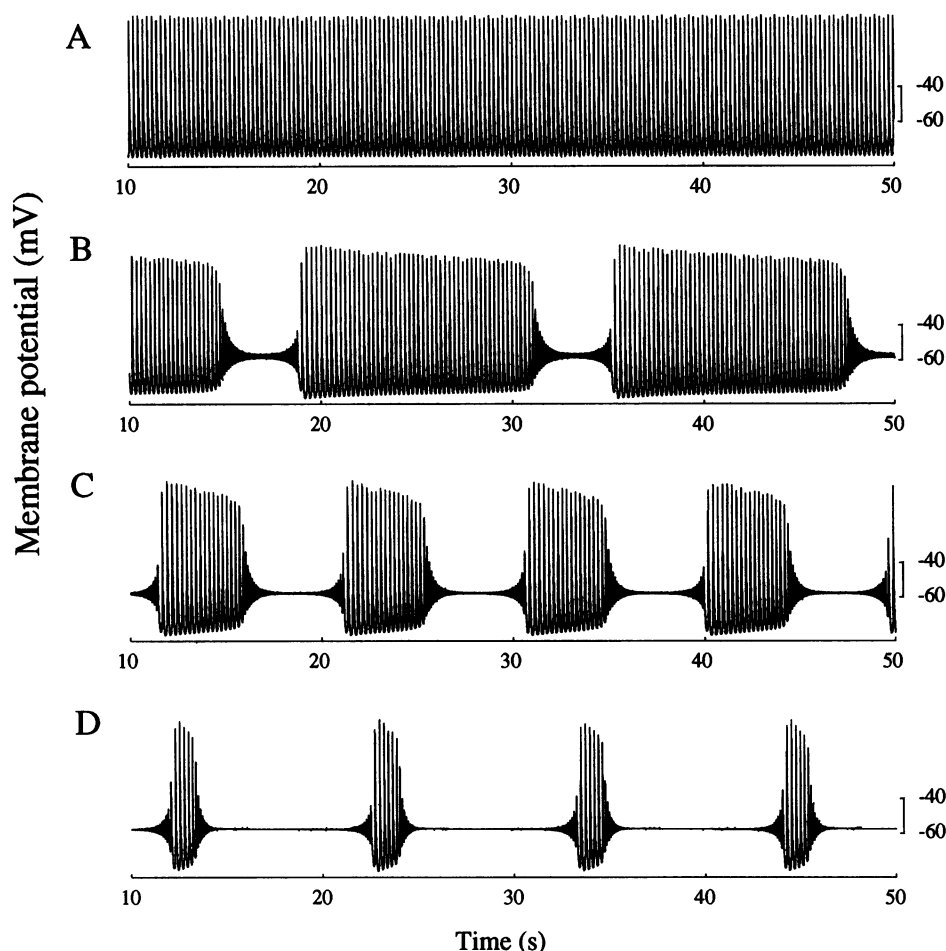


FIGURE 6 Transformation from slow oscillations to waxing and waning oscillations. The pattern of oscillations is shown for four values of  $\bar{g}_h$ . (A) slow oscillations ( $\bar{g}_h = 0.02$  mS/cm<sup>2</sup>). (B) A short silent phase interrupted the slow oscillation ( $\bar{g}_h = 0.021$  mS/cm<sup>2</sup>). (C) Oscillations with a longer silent phase ( $\bar{g}_h = 0.025$  mS/cm<sup>2</sup>). (D) For larger values of  $\bar{g}_h$ , the silent phase became more prominent ( $\bar{g}_h = 0.05$  mS/cm<sup>2</sup>).

that wax and wane, usually result from several oscillatory or stationary states. In this section, the dynamical states underlying waxing and waning oscillations are studied using a singular approximation method that identifies the origin and the transitions between these states.

Singular approximation is used in nonlinear dynamics to separate fast and slow subsystems (Pontryagin, 1961; Zeeman, 1973). Slow variables can be treated as slowly varying parameters and the rest of the system can then be studied as a function of these new parameters. This approximation has been successfully used to uncover the dynamical mechanisms underlying bursting oscillations in models of several biological systems (Rinzel, 1987).

We have applied this method to our model of waxing and waning oscillations. In Fig. 5, the gating variables  $S_2$  and  $F_2$  evolved according to a slower time scale than the other variables. In the case of  $I_{K2}$ -dependent waxing and waning oscillations (Fig. 9),  $S_1$  and  $h_2$  were the slow variables.

Let  $S_2$  be a slowly varying parameter in the  $\text{Ca}^{2+}$ -dependent model. In contrast,  $F_2$  only displays small variations of amplitude and therefore has a less prominent role

than  $S_2$ . As before, Eq. 6 was used for  $\text{Ca}^{2+}$ -dependent waxing and waning oscillations, except that  $S_2$  was assigned a constant value. In Fig. 5 A, since the variable  $S_2$  oscillates approximately between 0.09 and 0.65, the same interval of values will be used for  $S_2$  treated as a parameter.

Over this range of values, the system showed either a stable resting state or limit cycle oscillations (Fig. 10 A). For the smallest values of  $S_2$ , the system exhibited slow oscillations at a frequency of about 3.5 Hz, whereas for the highest values of the parameter  $S_2$ , the system exhibited a stable stationary state close to the depolarized resting state of Fig. 3 (around -57 mV).

The transition point between limit cycle oscillations and stable stationary state is called a *Hopf bifurcation* (Guckenheimer and Holmes, 1986; Rinzel and Ermentrout, 1989). In some cases, the stable solutions overlap, and the bifurcation is called *subcritical*. In our system, this transition has the typical structure of a subcritical Hopf bifurcation. First, the amplitude of the limit cycle at the bifurcation point changed abruptly and there was no decline in amplitude. Second, in some range of values of the parameter  $S_2$  (about 0.225–0.42),

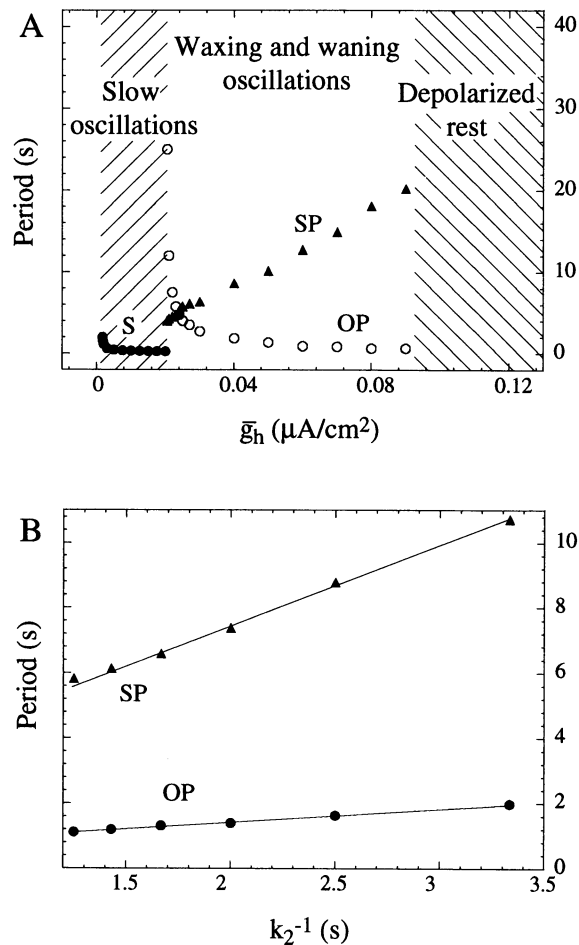


FIGURE 7 The period of  $\text{Ca}^{2+}$ -dependent waxing and waning oscillations depends on the maximal conductance of  $I_h$  and the time constant of  $\text{Ca}^{2+}$  binding to  $I_h$  channels. The length of the silent phase (SP) and the length of the oscillatory phase (OP) are shown as a function of these two parameters. (A) Period as a function of the maximal conductance of  $I_h$  ( $\bar{g}_h$ ). The range of values of  $\bar{g}_h$  corresponding to slow oscillations (period labeled by S), waxing and waning oscillations and depolarized resting state are also indicated. (B) Period as a function of the time constant ( $k_2^{-1}$ ) of intracellular  $\text{Ca}^{2+}$  binding on  $I_h$  channels. The inverse of the rate  $k_2$  is the time constant for  $\text{Ca}^{2+}$  binding.

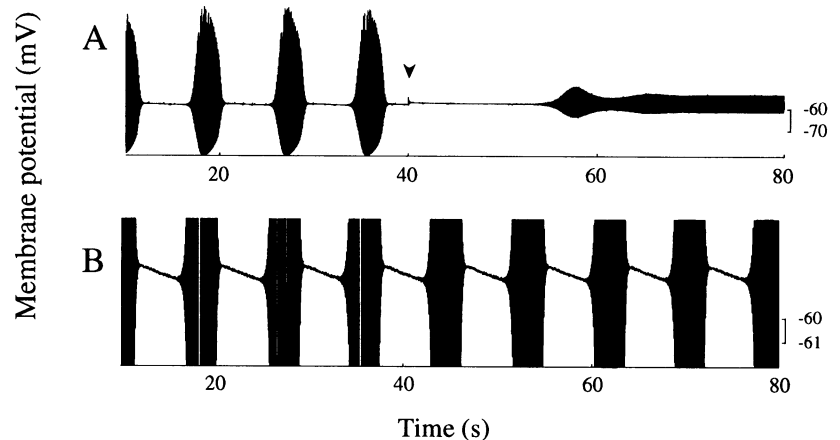
the stable limit cycle coexisted with the stable stationary state (Fig. 10 B). The state of the system within this interval of  $S_2$  depended on its previous history.

Thus, in a waxing and waning sequence,  $S_2$  oscillates between values which drive the system alternately between stable stationary states and slow oscillations. As shown by Fig. 10 B, the waxing and waning oscillations are driven around a hysteresis loop by the slow oscillations of  $S_2$ , as depicted by dotted arrows: as  $S_2$  decreases during the silent phase, the membrane potential hyperpolarizes slowly and follows the stable stationary state branch (arrow 1). As the critical point is reached, the stationary state loses its stability and the system jumps to the oscillating branch (arrow 2).  $S_2$  then starts to increase and follows the oscillating branch, while the amplitude of the oscillations decreases (arrow 3). The limit cycle oscillations lose stability and the system jumps back to the stationary branch (arrow 4). The oscillations damp and the silent phase starts again.

The trajectory of a simulated waxing and waning oscillation plotted in a  $V/S_2$  diagram, shown in Fig. 10 D, alternates between an oscillating and a stationary branch in a manner very similar to that in Fig. 10 B. The position of the oscillating and stationary branches seems to be slightly different from the solutions displayed in Fig. 10 B, but the structure remains the same. Waxing and waning oscillations with a longer oscillatory phase (see Fig. 6) correspond to a very similar trajectory, with an increased number of loops near the end of the oscillatory branch.

The same subcritical Hopf structure is still present for slow oscillations, but the successive loops do not leave the oscillatory branch and the oscillation does not wax and wane. A strong current pulse should, however, be able to make the trajectory jump from the oscillatory branch to the stationary branch. This prediction is borne out in Fig. 11, where a strong depolarizing current step induced a sudden transition to a silent phase during the slow oscillation (indicated by arrows 2 and 3 in Fig. 11 B) and the system returned back to the oscillatory branch (arrow 4) along a single hysteresis loop. Steps applied to  $S_2$  resulted in the same type of behavior.

FIGURE 8 Properties of  $I_{K2}$ -dependent waxing and waning oscillations. (A) Transformation of waxing and waning oscillations into slow oscillations by applying a depolarizing current step of  $0.24 \mu\text{A}/\text{cm}^2$  (arrow). (B) Waxing and waning oscillations at high amplification shows the slow hyperpolarization of the membrane during the silent phase.  $\bar{g}_h = 0.4 \text{ mS}/\text{cm}^2$ ,  $\bar{g}_{Ca} = 1.75 \text{ mS}/\text{cm}^2$ .



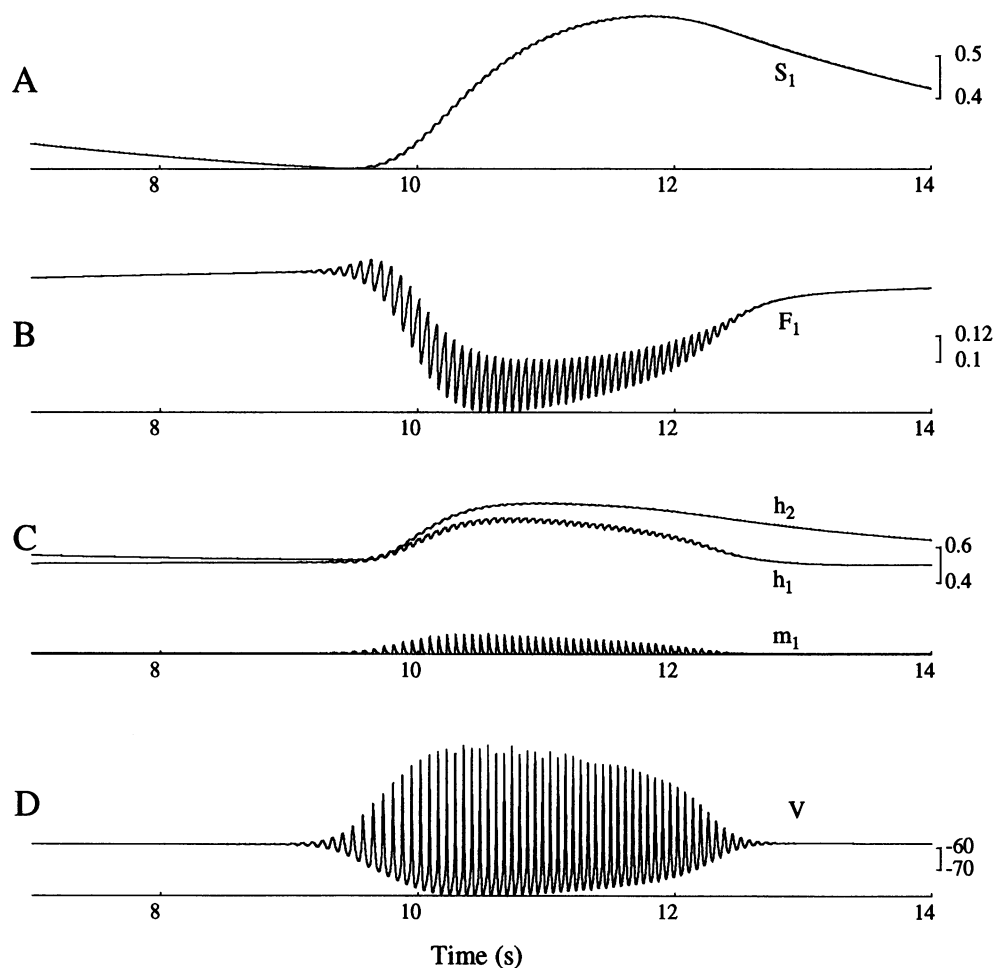


FIGURE 9 Time course of the gating variables of  $I_h$  and  $I_{K2}$  and the membrane potential during an  $I_{K2}$ -dependent waxing and waning oscillation. (A) Slow activation variable  $S_1$  of  $I_h$ . (B) Fast activation variable  $F_1$  of  $I_h$ . (C) Activation ( $m_2$ ) and inactivation ( $h_1$ ,  $h_2$ ) variables of  $I_{K2}$ . (D) Membrane potential  $V$ .  $\bar{g}_h = 0.4$  mS/cm<sup>2</sup>.

The same analysis can be applied to the  $I_{K2}$ -dependent waxing and waning oscillations, using  $S_1$  as a parameter. The  $I_{K2}$ -dependent waxing and waning oscillations were also based on a hysteresis loop around a subcritical Hopf bifurcation (not shown). The trajectory in the  $V/S_2$  diagram was very similar to the  $Ca^{2+}$ -dependent waxing and waning oscillations (Fig. 12).

## DISCUSSION

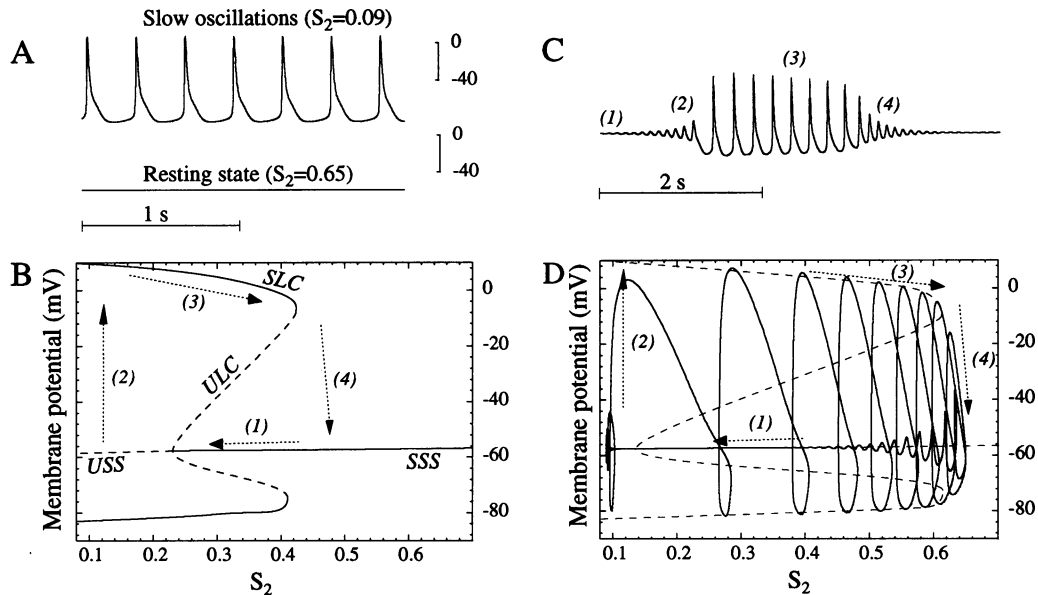
Hodgkin-Huxley-type models of TC neurons were first introduced by McMullen and Ly (1988) and Rose and Hindmarsh (1989) based on the experiments of Jahnsen and Llinas (1984a). More recent models of TC neurons (Destexhe and Babloyantz, 1993; Lytton and Sejnowski, 1992; McCormick and Huguenard, 1992; Toth and Crunelli, 1992a) take into account data from voltage-clamp experiments. We have extended these models by incorporating a more accurate model of  $I_h$  and have used it to study the genesis of waxing and waning oscillations that have been described in vitro (Leresche et al., 1990, 1991; Soltesz et al., 1991).

## The properties of $I_h$ in voltage-clamp mode

The hyperpolarization-activated inward current  $I_h$  is central to the oscillatory properties of TC neurons (McCormick and Pape, 1990a; Soltesz et al., 1991). First-order kinetic schemes have been proposed for modeling  $I_h$  in TC cells (Huguenard and McCormick, 1992; Lytton and Sejnowski, 1992; Toth and Crunelli, 1992a), sino-atrial node cells (DiFrancesco and Noble, 1985; van Ginneken and Giles, 1991) and stomatogastric ganglion neurons (Buchholtz et al., 1992); however, they do not reproduce the slow component of activation and the difference between activation and deactivation kinetics.

The model of  $I_h$  adopted here (Destexhe and Babloyantz, 1993) has two activation variables with different kinetics and accurately accounts for all the voltage-clamp data. Although more complex models have been developed for modeling a current similar to  $I_h$  in sino-atrial cells (DiFrancesco, 1985), the model used here is relatively simple and explains how slow activation can coexist with faster deactivation.

A  $Ca^{2+}$  dependence of  $I_h$  was included based on voltage-clamp measurements on sino-atrial node cells (Hagiwara and



**FIGURE 10** Singular approximation applied to the  $\text{Ca}^{2+}$ -dependent model of waxing and waning oscillations. (A) For extreme values of the slow variable  $S_2$  treated as a parameter, the system exhibited either slow oscillations ( $S_2 = 0.09$ ) or a stable stationary state ( $S_2 = 0.65$ ). Other parameters are the same as in Fig. 3 C. (B) Bifurcation diagram of the system as a function of  $S_2$ . During the slow oscillations of  $S_2$ , the system alternated between a slow oscillatory state and a resting state, tracing a hysteresis loop as shown in the diagram. The order of events underlying the waxing and waning sequence are indicated by dotted arrows. Dashed lines represent unstable states (USS, unstable stationary state; ULC, unstable limit cycle), and continuous lines represent stable states (SSS, stable stationary state; SLC, stable limit cycle). (C) Corresponding sequence of events in a single cycle of the waxing and waning oscillations. (D) Trajectories of waxing and waning oscillations in the  $V/S_2$  diagram. Here the full system was simulated without considering  $S_2$  as a parameter. Dashed lines represent the presumed position of oscillatory and stationary branches and dotted arrows depict the same sequence of events as in B.

Irisawa, 1989) and neocortical neurons (Schwindt et al., 1992). These data suggest that intracellular  $\text{Ca}^{2+}$  ions directly affect  $I_h$  channels and shift the activation function toward more depolarized potentials. We assumed that the  $\text{Ca}^{2+}$  dependence of  $I_h$  is caused by direct binding of  $\text{Ca}^{2+}$  ions on the open form of  $I_h$  channels (for a different model of this shift in the context of TC cells, see Toth and Crunelli (1992b)). Our model accounts for the positive shift of the activation function of  $I_h$  with increased intracellular  $\text{Ca}^{2+}$ , but not for the substantial increase of conductance. It should be possible to verify the predicted logarithmic shift (Eq. 12) from whole cell patch-clamp experiments.

### Combinations of currents giving rise to waxing and waning oscillations

The properties of waxing and waning oscillations (Leresche et al., 1991) were reproduced by our model, which included  $I_T$  and  $\text{Ca}^{2+}$ -dependent  $I_h$ . The silent phase was many seconds long, during which the membrane potential slowly hyperpolarized. A transition to periodic oscillations could be elicited by application of a depolarizing current step only for some values of the parameter  $\bar{g}_h$ . Experimental studies report this transition in only two out of 39 cat TC cells (Leresche et al., 1991).

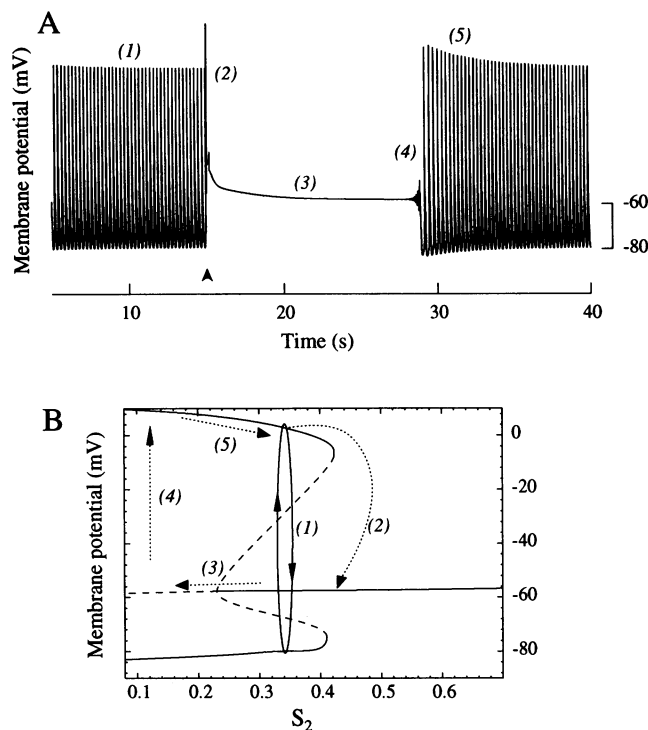
More importantly, the sequence of resting and oscillatory behavior obtained was identical to that determined in vitro (Soltesz et al., 1991). In these experiments, noradrenaline (NE) was used to change  $I_h$ , but NE also shifts the activation

function of  $I_h$  by a few millivolts (McCormick and Pape, 1990b). We did not include this shift in our simulations.

We also found intermediate patterns of oscillations which were not reported experimentally. Close to the transition between slow oscillations and waxing and waning oscillations there were long oscillatory phases and short silent phases. TC cells in vitro show a variety of patterns of waxing and waning oscillations with silent and oscillatory phases of different lengths. The range of patterns found in the model for different values of the parameters suggests that the variability observed in vitro might arise from a heterogeneity of the conductance values among neurons.

We also investigated the occurrence of waxing and waning oscillations in a model comprising  $I_T$ ,  $I_h$ , and the slow  $\text{K}^+$  current  $I_{K2}$  (Destexhe and Babloyantz, 1993). The main difference was that the frequency inside the oscillatory phase was significantly higher in  $I_{K2}$ -dependent waxing and waning oscillations (10–14 Hz) compared to the same oscillations obtained from the  $\text{Ca}^{2+}$ -dependent mechanism (3.5–4 Hz). The frequency of oscillations in the  $\text{Ca}^{2+}$ -dependent model was much closer to the experimental data of Leresche et al. (1991).

In the case of the  $\text{Ca}^{2+}$ -dependent model, the waxing and waning oscillations were modulated by the kinetics of binding of  $\text{Ca}^{2+}$ , whereas, in the case of the  $I_{K2}$ -dependent model, they appear to be modulated by the slow activation of  $I_h$ . Although the values of  $I_T$  and leakage parameters were the same, 10-fold higher values of  $\bar{g}_h$  were needed to observe similar types of behavior for the  $I_{K2}$ -dependent model.



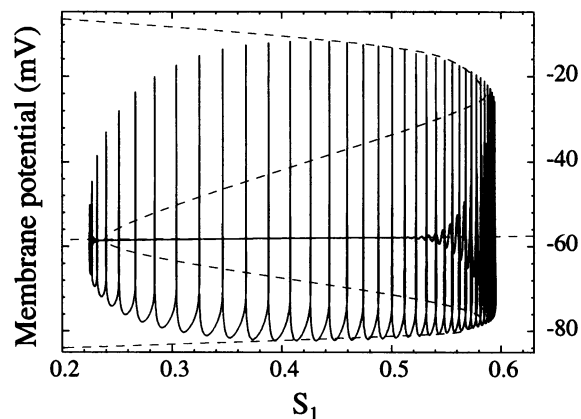
**FIGURE 11** Induction of a silent phase during slow oscillations. (A) A strong depolarizing current pulse of 200 ms and  $10 \mu\text{A}/\text{cm}^2$  ( $0.1 \text{ nA}$ ) (arrow) damps the slow oscillation for several seconds until spontaneously reappearing. Same parameters as in Fig. 6 A. (B) Same sequence of events illustrated in a  $V/S_2$  diagram. The stable and unstable branches are as described in Fig. 10 B; the closed curve (1) represents the slow oscillation limit cycle and the dotted arrows (2–5) indicate the sequence of events induced by the current pulse. The same sequence of events is reported in A.

$\text{Ca}^{2+}$ -dependent waxing and waning oscillations were also observed in the presence of fast  $\text{Na}^+$  and  $\text{K}^+$  currents responsible for action potentials (unpublished; kinetics taken from Traub and Miles (1991)). In this case, waxing and waning oscillations occurred as sequences of rhythmic bursting (3.5–4 Hz; fast spikes at 50–300 Hz) separated by long silent phases (4–30 s).

### Dynamical mechanisms of waxing and waning oscillations

Singular approximation was used to characterize the waxing and waning oscillation as an alternation between two dynamical states, a hyperpolarizing stationary phase and an oscillating phase. The transitions between these two states were made via a subcritical Hopf bifurcation. It was remarkable that the same dynamical mechanism underlies both the  $\text{Ca}^{2+}$ -dependent and the  $I_{\text{K}2}$ -dependent models, despite the different ionic mechanisms.

A similar type of dynamical mechanism was proposed previously by Rinzel (1987) for the Fitzhugh-Nagumo equations (Fitzhugh, 1961), in which a subcritical Hopf bifurcation emerged from a stationary state, leading to bursting oscillations. The same subcritical Hopf structure was also present during slow oscillations. We found that a strong depolarizing



**FIGURE 12** Trajectories of waxing and waning oscillations for  $I_{\text{K}2}$ -dependent waxing and waning oscillations. The same type of diagram as Fig. 10 D is constructed with  $V$  plotted against  $S_1$  (same parameters as in Fig. 9). Dashed lines are the presumed positions of oscillatory and stationary branches.

current pulse of 200 ms can force the TC cell out of the oscillatory phase for a period of about 15 s before the cells reverts back to slow oscillations. However, weaker current pulses do not produce such an interruption but only affect the phase of the slow oscillations (not shown). This prediction of the model could be tested experimentally.

### The role of $I_h$

Soltesz et al. (1991) suggested that slow oscillations and waxing and waning rhythmicity observed in vitro correspond to two different equilibria between  $I_T$  and  $I_h$ . The results presented here are consistent with this hypothesis.

The pattern of oscillations depended on the value of the maximal conductance of  $I_h$  and slowly varying this parameter smoothly transforms the slow oscillations into waxing and waning oscillations. This suggests that slow oscillations and waxing and waning oscillations are part of a continuum of oscillating states that can be determined in part by the maximal conductance of  $I_h$ .

The  $\text{Ca}^{2+}$ -dependent waxing and waning oscillations were insensitive to the details of the kinetics of the models for  $I_T$  and for the kinetics of binding of intracellular  $\text{Ca}^{2+}$  on  $I_h$  channels. However, when  $\text{Ca}^{2+}$  binding to  $I_h$  was modeled by a simple activation scheme (Huguenard and McCormick, 1992) rather than the double activation model (Destexhe and Babloyantz, 1993), then waxing and waning oscillations were not observed over a wide range of parameter values. These results suggest that the description of  $I_h$  by double activation kinetics might be important for robustly generating waxing and waning patterns of oscillation, but more evidence is needed to demonstrate this point.

### Implications for the physiology of thalamic oscillations

Our model suggests that interactions between  $I_T$ ,  $I_h$ , and the leakage currents are the kernel that allows the coexistence of

tonic firing, slow oscillations, and waxing and waning oscillations in TC cells. Experiments can be designed to test which of the two proposed mechanisms is responsible for the oscillations. The higher frequency of the  $I_{K2}$ -dependent model makes it less plausible than the  $\text{Ca}^{2+}$ -dependent model. The  $I_{K2}$ -dependent model predicts that the waxing and waning oscillations should not survive blockage of all voltage-dependent  $\text{K}^+$  currents (but not the leak  $\text{K}^+$  currents, needed to maintain the level of membrane potential). The  $\text{Ca}^{2+}$ -dependent model could be tested by altering the intracellular  $\text{Ca}^{2+}$  levels while monitoring the period of waxing and waning oscillations. The  $\text{Ca}^{2+}$ -dependent model predicts that this period should be sensitive to intracellular  $\text{Ca}^{2+}$ .

The intrinsic oscillating properties of TC cells are difficult to reconcile with the various types of oscillations found in vivo (Nunez et al., 1992). The occurrence of spindling in vivo is thought to be a combination of intrinsic and network properties (Steriade and Llinas, 1988; Steriade et al., 1993b). In particular, single thalamic reticular cells are characterized by 7–12-Hz intrinsic oscillations (Avanzini et al., 1989; Bal and McCormick, 1993), close to the typical frequency of sleep spindles. Spindle rhythmicity was also found in the isolated reticular thalamus in vivo (Steriade et al., 1987). On the other hand, TC cells have a clear tendency to oscillate at a lower frequency of 0.5–4 Hz (Curró Dossi et al., 1992; Leresche et al., 1990, 1991; McCormick and Pape, 1990a) and have been shown to have an active role in the generation of spindles in vitro (von Krosigk et al., 1993). Computer models of the intrinsic oscillatory properties of thalamic reticular and TC cells, as well as their pattern of connectivity, could help us to understand the cellular bases of spindling (Destexhe et al., 1993a,b).

We thank Drs. Diego Contreras, John Huguenard, William Lytton, David McCormick and Mircea Steriade for stimulating discussions.

This research was supported by the Belgian government (ARC and IMPULS, project RFO AI 10), the European Community (ESPRIT, Basic Research, project 3234), the Howard Hughes Medical Institute, and the United States Office of Naval Research.

## REFERENCES

- Avanzini, G., M. de Curtis, F. Panzica, and R. Spreafico. 1989. Intrinsic properties of nucleus reticularis thalami neurones of the rat studied in vitro. *J. Physiol. (Lond.)*. 416: 111–122.
- Bal, T., and D. A. McCormick. 1993. Mechanisms of oscillatory activity in guinea-pig nucleus reticularis thalami in vitro: a mammalian pacemaker. *J. Physiol. (Lond.)*. 468:669–691.
- Blaustein, M. P. 1988. Calcium transport and buffering in neurons. *Trends Neurosci.* 11:438–443.
- Buchholtz, F., J. Golowasch, I. R. Epstein, and E. Marder. 1992. Mathematical model of an identified stomatogastric ganglion neuron. *J. Neurophysiol.* 67:332–340.
- Budde, T., R. Mayer, and H. C. Pape. 1992. Different types of potassium outward current in relay neurons acutely isolated from the rat lateral geniculate nucleus. *Eur. J. Neurosci.* 4:708–722.
- Coulter, D. A., J. R. Huguenard, and D. A. Prince. 1989. Calcium currents in rat thalamocortical relay neurones: kinetic properties of the transient, low-threshold current. *J. Physiol. (Lond.)*. 414:587–604.
- Crunelli, V., S. Lightowler, and C. E. Pollard. 1989. A T-type  $\text{Ca}^{2+}$  current underlies low-threshold  $\text{Ca}^{2+}$  potentials in cells of the cat and rat lateral geniculate nucleus. *J. Physiol. (Lond.)*. 413:543–561.
- Curró Dossi, R., A. Nunez, and M. Steriade. 1992. Electrophysiology of a slow (0.5–4 Hz) intrinsic oscillation of cat thalamocortical neurones in vivo. *J. Physiol. (Lond.)*. 447:215–234.
- Deschênes, M., M. Paradis, J. P. Roy, and M. Steriade. 1984. Electrophysiology of neurons of lateral thalamic nuclei in cat: resting properties and burst discharges. *J. Neurophysiol.* 55:1196–1219.
- Destexhe, A., and A. Babloyantz. 1993. A model of the inward current  $I_h$  and its possible role in thalamocortical oscillations. *NeuroReport*. 4:223–226.
- Destexhe, A., W. W. Lytton, T. J. Sejnowski, D. A. McCormick, D. Contreras, and M. Steriade. 1993a. A model of 7–14 Hz spindling in the thalamus and thalamic reticular nucleus: interaction between intrinsic and network properties. *Soc. Neurosci.* 19:516.
- Destexhe, A., D. A. McCormick, and T. J. Sejnowski. 1993b. A model of 8–10 Hz spindling in interconnected thalamic relay and reticularis neurones. *Biophys. J.* In press.
- DiFrancesco, D. 1985. The cardiac hyperpolarization-activated current  $I_h$ , origins and developments. *Prog. Biophys. Mol. Biol.* 46:163–183.
- DiFrancesco, D., and D. Noble. 1985. A model of cardiac electrical activity incorporating ionic pumps and concentration changes. *Philos. Trans. R. Soc. Lond. B Biol. Sci.* 307:353–398.
- Erickson, K. R., O. K. Ronnekleiv, and M. J. Kelly. 1993. Electrophysiology of guinea-pig supraoptic neurones: role of a hyperpolarization-activated cation current in phasic firing. *J. Physiol. (Lond.)*. 460:407–425.
- Fitzhugh, R. 1961. Impulses and physiological states in models of nerve membrane. *Biophys. J.* 1:445–466.
- Galligan, J. J., H. Tatsumi, K. Z. Shen, A. Surprenant, and R. A. North. 1990. Cation current activated by hyperpolarization ( $I_h$ ) in guinea pig enteric neurons. *Am. J. Physiol.* 259:G966–972.
- Guckenheimer, J., and P. Holmes. 1986. Nonlinear Oscillations, Dynamical Systems and Bifurcations of Vector Fields. Springer, Berlin. 459 pp.
- Haby, M., N. Leresche, D. Jassik-Gerschenfeld, I. Soltesz, and V. Crunelli. 1988. Spontaneous rhythmic depolarizations in projection cells of the rat lateral geniculate nucleus in vitro: role of NMDA receptors. *C. R. Acad. Sci. Paris Ser. III.* 306:195–199.
- Hagiwara, N., and H. Irisawa. 1989. Modulation by intracellular  $\text{Ca}^{2+}$  of the hyperpolarization-activated inward current in rabbit single sino-atrial node cells. *J. Physiol. (Lond.)*. 409:121–141.
- Hines, M. 1989. A program for simulation of nerve equations with branching geometries. *Int. J. Biomed. Comput.* 24:55–68.
- Hines, M. 1993. NEURON—a program for simulation of nerve equations. In *Neural Systems: Analysis and Modeling*. F. Eeckman, editor. Kluwer Academic Publishers. Norwell, MA. 127–136.
- Hodgkin, A. L., and A. F. Huxley. 1952. A quantitative description of membrane current and its application to conduction and excitation in nerve. *J. Physiol. (Lond.)*. 117:500–544.
- Huguenard, J. R., and D. A. McCormick. 1992. Simulation of the currents involved in rhythmic oscillations in thalamic relay neurons. *J. Neurophysiol.* 68:1373–1383.
- Huguenard, J. R., and D. A. Prince. 1992a. Slow inactivation of a TEA-sensitive K current in acutely isolated rat thalamic relay neurons. *J. Neurophysiol.* 66:1316–1328.
- Huguenard, J. R., and D. A. Prince. 1992b. A novel T-type current underlies prolonged  $\text{Ca}^{2+}$ -dependent bursts firing in GABAergic neurons of rat thalamic reticular nucleus. *J. Neurosci.* 12:3804–3817.
- Jahnsen, H., and R. R. Llinas. 1984a. Electrophysiological properties of guinea-pig thalamic neurons: an in vitro study. *J. Physiol. (Lond.)*. 349:205–226.
- Jahnsen, H., and R. R. Llinas. 1984b. Ionic basis for the electroresponsiveness and oscillatory properties of guinea-pig thalamic neurons in vitro. *J. Physiol. (Lond.)*. 349:227–247.
- Kamondi, A., and P. B. Reiner. 1991. Hyperpolarization-activated inward current in histaminergic tuberomammillary neurons of the rat hypothalamus. *J. Neurophysiol.* 66:1902–1911.
- Leresche, N., D. Jassik-Gerschenfeld, M. Haby, I. Soltesz, and V. Crunelli. 1990. Pacemaker-like and other types of spontaneous membrane potential oscillations in thalamocortical cells. *Neurosci. Lett.* 113:72–77.
- Leresche, N., S. Lightowler, I. Soltesz, D. Jassik-Gerschenfeld, and V. Crunelli. 1991. Low frequency oscillatory activities intrinsic to rat and cat thalamocortical cells. *J. Physiol. (Lond.)*. 441:155–174.

- Lytton, W. W., and T. J. Sejnowski. 1992. Computer model of ethosuximide's effect on a thalamic cell. *Ann. Neurol.* 32:131–139.
- McCormick, D. A. 1991. Functional properties of a slowly inactivating potassium current in guinea-pig dorsal lateral geniculate relay neurons. *J. Neurophysiol.* 66:1176–1189.
- McCormick, D. A. 1992. Neurotransmitter actions in the thalamus and cerebral cortex and their role in neuromodulation of thalamocortical activity. *Prog. Neurobiol.* 39:337–388.
- McCormick, D. A., and J. R. Huguenard. 1992. A model of the electrophysiological properties of thalamocortical relay neurons. *J. Neurophysiol.* 68:1384–1400.
- McCormick, D. A., and H. C. Pape. 1990a. Properties of a hyperpolarization-activated cation current and its role in rhythmic oscillations in thalamic relay neurones. *J. Physiol. (Lond.)*. 431:291–318.
- McCormick, D. A., and H. C. Pape. 1990b. Noradrenergic modulation of a hyperpolarization-activated cation current in thalamic relay neurones. *J. Physiol. (Lond.)*. 431:319–342.
- McCormick, D. A., and A. Williamson. 1991. Modulation of neuronal firing mode in cat and guinea pig LGNd by histamine: possible cellular mechanisms of histaminergic control of arousal. *J. Neurosci.* 11:3188–3199.
- McMullen, T. A., and N. Ly. 1988. Model of oscillatory activity in thalamic neurons: role of voltage and calcium-dependent ionic conductances. *Biol. Cybernet.* 58:243–259.
- Nunez, A., R. Curro Dossi, D. Contreras, and M. Steriade. 1992. Intracellular evidence for incompatibility between spindle and delta oscillations in thalamocortical neurons of cat. *Neuroscience*. 48:75–85.
- Pape, H. C. 1992. Adenosine promote burst activity in guinea-pig geniculocortical neurones through two different ionic mechanisms. *J. Physiol. (Lond.)*. 447:729–753.
- Pollard, C. E., and V. Crunelli. 1988. Intrinsic membrane currents in projection cells of the cat and rat lateral geniculate nucleus. *Neurosci. Lett.* 32:S39.
- Pontryagin, L. S. 1961. Asymptotic behavior of the solutions of systems of differential equations with a small parameter in the higher derivatives. *Am. Math. Soc. Trans. Sec. II.* 18:275–290.
- Press, W. H., B. P. Flannery, S. A. Teukolsky, and W. T. Vetterling. 1986. Numerical Recipes. The Art of Scientific Computing. Cambridge University Press, Cambridge. 735 pp.
- Rinzel, J. 1987. A formal classification of bursting mechanisms in excitable systems. In *Mathematical Topics in Population Biology, Morphogenesis and Neurosciences*. E. Teramoto and M. Yamaguti, editors. Springer-Verlag, Berlin. 267–281.
- Rinzel, J., and G. B. Ermentrout. 1989. Analysis of neural excitability and oscillations. In *Methods in Neuronal Modeling*. C. Koch and I. Segev, editors. MIT press, Cambridge, MA. 135–169.
- Rose, R. M., and J. L. Hindmarsh. 1989. The assembly of ionic currents in a thalamic neuron. I. The three-dimensional model. *Proc. R. Soc. Lond. B Biol. Sci.* 237:267–288.
- Schwindt, P. C., W. J. Spain, and W. E. Crill. 1992. Effects of intracellular calcium chelation on voltage-dependent and calcium-dependent currents in cat neocortical neurons. *Neuroscience*. 47:571–578.
- Soltesz, I., S. Lightowler, N. Leresche, D. Jassik-Gerschenfeld, C. E. Pollard, and V. Crunelli. 1991. Two inward currents and the transformation of low frequency oscillations of rat and cat thalamocortical cells. *J. Physiol. (Lond.)*. 441:175–197.
- Steriade, M., and M. Deschênes. 1984. The thalamus as a neuronal oscillator. *Brain Res. Rev.* 8:1–63.
- Steriade, M., and R. R. Llinas. 1988. The functional states of the thalamus and the associated neuronal interplay. *Physiol. Rev.* 68:649–742.
- Steriade, M., M. Deschênes, L. Domich, and C. Mulle. 1985. Abolition of spindle oscillations in thalamic neurons disconnected from nucleus reticularis thalami. *J. Neurophysiol.* 54:1473–1497.
- Steriade, M., L. Domich, G. Oakson, and M. Deschênes. 1987. The deaf-ferented reticular thalamic nucleus generates spindle rhythmicity. *J. Neurophysiol.* 57:260–273.
- Steriade, M., P. Gloor, R. R. Llinas, F. H. Lopes da Silva, and M. M. Mesulam. 1990. Basic mechanisms of cerebral rhythmic activities. *EEG Clin. Neurophysiol.* 76:481–508.
- Steriade, M., E. G. Jones, and R. R. Llinas. 1990. *Thalamic Oscillations and Signalling*. John Wiley & Sons, New York. 431 pp.
- Steriade, M., D. Contreras, R. Curró Dossi, and A. Nunez. 1993a. The slow (<1 Hz) oscillation in reticular thalamus and thalamocortical neurons. Scenario of sleep rhythms generation in interacting thalamic and neocortical networks. *Neuroscience*. 13:3284–3299.
- Steriade, M., D. A. McCormick, and T. J. Sejnowski. 1993b. Thalamocortical oscillations in the sleeping and aroused brain. *Science (Wash. DC)*. In press.
- Toth, T., and V. Crunelli. 1992a. Computer simulations of the pacemaker oscillations of thalamocortical cells. *NeuroReport*. 3:65–68.
- Toth, T., and V. Crunelli. 1992b. Modelling spindle-like oscillations in thalamocortical neurones. *Soc. Neurosci. Abstr.* 18:1018.
- Traub, R. D., and R. Miles. 1991. *Neuronal Networks of the Hippocampus*. Cambridge University Press, Cambridge. 281 pp.
- Uchimura, N., E. Cherubini, and R. A. North. 1990. Cation current activated by hyperpolarization in a subset of rat nucleus accumbens neurons. *J. Neurophysiol.* 64:1847–1850.
- van Ginneken, A. C. G., and W. Giles. 1991. Voltage-clamp measurements of the hyperpolarization-activated inward current  $I_f$  in single cells from rabbit sino-atrial node. *J. Physiol. (Lond.)*. 434:57–83.
- von Krosigk, M., T. Bal, and D. A. McCormick. 1993. Cellular mechanisms of a synchronized oscillation in the thalamus. *Science (Wash. DC)*. 261:361–364.
- Wang, X. J., J. Rinzel, and M. A. Rogawski. 1991. A model of the T-type calcium current and the low-threshold spike in thalamic neurons. *J. Neurophysiol.* 66:839–850.
- Zeeman, E. C. 1973. Differential equations for the heart beat and nerve impulse. In *Dynamical Systems*. M. Peixoto, editor. Academic Press, New York. 683–741.